http://aojnmb.mums.ac.ir

AOJNM

Quantification of bone metabolic activity in the natural course of fractural lesions measured by quantitative SPECT/CT

Tomohiko Yamane^{1, 2*}, Yohji Matsusaka², Kenji Fukushima^{2, 3}, Akira Seto², Ichiro Matsunari⁴, Ichiei Kuji²

¹Department of Molecular Imaging Research, Kobe City Medical Center General Hospital, Japan ²Department of Nuclear Medicine, Saitama Medical University International Medical Center, Japan ³Department of Radiology and Nuclear Medicine, Fukushima Medical University, Japan ⁴Division of Nuclear Medicine, Department of Radiology, Saitama Medical University Hospital, Japan

ARTICLEINIO ADJIRACI
Article type:Objective(s):While increased uptake at the bone fractural site gradually decreases over time on bone scans, the rate of change has not been quantitatively evaluated. The purpose of this study was to quantify the extent of bone metabolic changes in
Article history: Received: 7 Feb 2022 Revised: 25 Mar 2022 Accepted: 3 Apr 2022fractural lesions on bone SPECT/CT. Methods: We reviewed bone scans acquired by dedicated SPECT/CT and chose those scans in which quantitative SPECT/CT of the same range was acquired twice or more. We set the region of interest on lesions of bone fracture and degeneration, and measured the maximum standardized uptake value (SUVmax). From the SUVmax
<i>Keywords:</i> Bone fractures Single photon emission computed tomography Radionuclide imaging Quantification Standardized uptake value Keywords: Bone fractures Single photon emission computed tomography Radionuclide imaging Quantification Standardized uptake value Keywords: Keyw

Please cite this paper as:

Yamane T, Matsusaka Y, Fukushima K, Seto A, Matsunari I, Kuji I. Quantification of bone metabolic activity in the natural course of fractural lesions measured by quantitative SPECT/CT. Asia Ocean J Nucl Med Biol. 2023; 11(1): 30-36. doi: 10.22038/A0JNMB.2022.63484.1446

Introduction

Bone scans show increased tracer uptake in fractural lesions. When evaluating bone metastasis, uptake in the fracture occasionally

interrupts precise diagnosis, especially for solitary lesions (1). Accumulation at fractural sites is well known to gradually decrease (2),

^{*} Corresponding author: Tomohiko Yamane. Division of Molecular Imaging Research, Kobe City Medical Center General Hospital Minatojima-Minamimachi 2-1-1, Chuo-Ku, Kobe, 650-0047, Japan. Tel: +81-78-302-4321; E-mail: tomohiko_yamane@kcho.jp

^{© 2023} mums.ac.ir All rights reserved.

This is an Open Access article distributed under the terms of the Creative Commons Attribution License (http://creativecommons.org/licenses/by/3.0), which permits unrestricted use, distribution, and reproduction in any medium, provided the original work is properly cited.

and this decline can be one of the keys to differentiating fractural lesions from malignant lesions. However, how fast the accumulation decreases over time has not been characterized objectively.

Recent advances in single photon emission computed tomography (SPECT) have been improving quantitative technology (3, 4). In addition to software-based methods (5), hardware-based techniques combined with computed tomography (CT) can accurately calculate quantitative values (6). Standardized (SUV), uptake value a representative quantitative value used initially in positron emission tomography (PET), has also been used in SPECT quantification. Using SUV calculated from quantitative SPECT/CT systems, we can discriminate bone metastases from benign lesions (7). In addition, SUV from bone SPECT can be used to diagnose various benign diseases (8, 9) and evaluate physiological bone metabolism (10) as well as monitor the effects of treatment in cancer therapy (11).

Clarification of quantitative changes in the bone metabolism of fractural lesions is essential to understand the pathogenesis of bone metabolism. The changes observed in fractures are expected to differ from those involved in degenerative lesions, which also often show positive accumulation on bone scans. The purpose of this study was therefore to describe the extent of bone metabolic changes in fractural lesions observed by bone scintigraphy.

Methods

Patients

The protocol for this retrospective study was approved by the institutional review board of Medical University International Saitama Medical Center (approval no. #20-056), and the need for written informed consent was waived. We reviewed all clinical images from bone scans acquired between August 2017 and April 2020 from a dedicated SPECT/CT platform (Symbia Intevo; Siemens, Erlangen, Germany). We included only those cases in which quantitative SPECT/CT of the same range was acquired at least twice. Among those, we excluded scans showing extravascular tracer leakage or insufficient image quality for the calculation of quantitative values. We also eliminated from analysis those scans showing no apparent fracture or degeneration. In addition, while we used two kinds of tracers for bone scans, scans that used different tracers were also avoided in the analysis.

SPECT/CT and quantification

Patients received approximately 740 MBq of

^{99m}Tc-methylene diphosphonate (^{99m}Tc-MDP) or ^{99m}Tc-hydroxymethylene diphosphonate (^{99m}Tc-HMDP). Approximately three hours after injection of the tracer, SPECT/CT images were acquired using the integrated SPECT/CT scanner (Symbia Intevo; Siemens, Erlangen, Gernamy). Parameters for SPECT were: continuous rotation mode; acquisition, 180° for each head with a noncircular orbit; energy peak, 140 keV with 15% width; projection, 60 views over 180° with a dwell time of 10 s/view (total, 10 min/bed position); reconstruction, ordered subset conjugate gradient minimizer algorithm with one subset and 48 iterations; preset mode with scatter and attenuation corrections, "enhanced" and "skeletal" (xSPECT Bone; Siemens); matrix, 2.54×2.54×2.54 mm; and pixel size, 256×256. Furthermore, parameters for the CT were: voltage, 130 kV; tube current, automatic dose modulation (Care Dose 4D; Siemens) with a set reference current of 60 mAs; tube rotation time, 0.6 s; pitch, 1.0; and matrix, 512×512.

Image analysis

Two board-certified nuclear medicine physicians evaluated lesions showing increased uptake on SPECT images and chose those lesions considered to represent either fracture or degeneration by consensus. The physicians drew regions of interest (ROIs) on a workstation for nuclear medicine (syngo.via NM Oncology WF for VA 30; Siemens), and SUV was calculated by the following equation:

$$SUV = \frac{Activity \ concentration \ (Bq/ml) \times Body \ weight \ (g)}{Injected \ radioactivity \ (Bq)}$$

In the analysis, SUV_{max} was used offering maximal SUV from the pixels within the ROI. The ROI was manually drawn on follow-up images in the same area as in the first scan, and SUV_{max} was measured.

Statistical analysis

For a bone scan image in which a fractural or degenerative lesion was present, we examined all other follow-up scans in which the same lesion was observable and recorded the SUV_{max} of each lesion and the interval in days between scans. If scans were performed three times or more, data were recorded between all combinations, i.e., when three scans were performed, data were recorded three times; between the first and second scans, between the first and third scans, and between the second and third scans. In cases where abnormal uptake disappeared during follow-up, we did not include the case in subsequent analyses. То facilitate an understanding of the rate of change, standardized values for the 30-day rate of change

 $\Delta SUV_{max}30d)$ were calculated using the following formula,

$$\Delta SUVmax30d = \frac{postSUVmax - preSUVmax}{days between the scans} \times 30,$$

where $postSUV_{max}$ and $preSUV_{max}$ indicate SUV_{max} at the later and earlier scans, respectively.

We evaluated how much SUV_{max} of the day changed after 30 days utilizing a linear leastsquares method on fractural and degenerative lesions by comparing the relationship between preSUV_{max} and Δ SUV_{max}30d. In addition, we evaluated the ability to differentiate between fracture and degeneration by receiver operating characteristics (ROC) analysis and the Mann-Whitney *U* test. Areas under the curve (AUCs) were calculated for ROC analysis. These differential abilities were analyzed in all cases and the following five groups for preSUV_{max} were defined: 30≤ preSUV_{max}, 20≤ preSUV_{max} <30, 15≤ $preSUV_{max}$ <20, 10≤ $preSUV_{max}$ <15, and preSUV_{max} <10. Values of *p* <0.05 were considered statistically significant. We used integrated statistical software (Prism 8.4.3; GraphPad

Table 1. Patient characteristics

Software, San Diego, CA, USA).

Results

Patients and analyzed lesions

Among patients who underwent bone SPECT/CT scan twice or more, we reviewed 666 bone SPECT/CT scans from 206 patients. A total of 19 scans met the exclusion criteria, comprising 18 scans with extravascular leakage of tracer and 1 scan with insufficient image quality. We also excluded a further eight scans in which paired scans were unavailable. Moreover, we excluded 464 cases in which no fracture or degeneration lesions were evident. As a result, we finally included and analyzed 175 scans from 60 patients in this study. Table 1 summarizes detailed patients characteristics. Among these, we identified 157 combinations for fractural lesions and 266 combinations for degenerative lesions. Table 2 summarizes the detailed characteristics of these combinations. None of these combinations of scans used different tracers. Figure 1 shows representative cases.

Number		60
Age (patient-based)	Range, median	44–86, 73.5
Sex	Men	54
(patient-based)	Women	6
Tracer for bone scan	*99mTc-MDP	54
(patient-based)	**99mTc-HMDP	6
Primary disease for bone scan (patient-based)	Prostate cancer	52
	Breast cancer	4
	Renal cell carcinoma	2
	Gastric cancer	1
	Thyroid cancer	1
Total lesions analyzed	Fracture	66
	Degeneration	77

*99mTc-MDP, 99mTc-methylene diphosphonate; ** 99mTc-HMDP, 99mTc-hydroxymethylene diphosphonate

Table 2. Characteristics of analyzed combinations between two scans

Analyzed scan combinations	Fracture	157	
Analyzeu scan combinations	Degeneration	266	
Interval between scans (days)	Fracture (range, median)	24-822, 176	
Interval between scans (days)	Degeneration (range, median)	28-886, 261.5	
	Rib	122	
Fractural lesions (combination-based)	Vertebra	23	
	Clavicle	6	
	Pelvis	4	
	Sternum	2	
Degenerative lesions	Vertebra including osteophyte and adjacent joint	210	
(combination-based) Around joint in the chest area		56	



Figure 1. Maximum intensity projections, fused SPECT/CT, and CT images of representative cases; first scan (a) and the follow-up scan after 155 days (b) in fractural lesions, and first scan (c) and the follow-up scan after 169 days (d) in degenerative lesions. SUV_{max} of bone fracture in the sternum changed from 30.0 to 6.2, and in the left fifth rib changed from 17.2 to 4.6 (**arrowheads**). Bone metastases are also visualized as intensively increased uptake in the pubis and ischium (**arrows**). SUV_{max} of degeneration in the Th12 osteophyte changed from 19.4 to 20.7, and in the left lumbosacral facet joint changed from 18.8 to 22.9 (**arrowheads**). The color scale in the fused SPECT/CT images is illustrated on the right side of this figure ranged SUV 0—15. SUV, Standardized uptake value; SUV_{max}, maximum SUV

F

D

Regression Analysis

Scatterplots of the relationship between preSUV_{max} and Δ SUV_{max}30d are shown in Figure 2. For fractural legions, the formula was as follows:

 $\Delta SUVmax30d = -0.15 \times preSUVmax + 1.35.$

With this formula, the 95%CI of the slope was -0.17 to -0.13, and the intercept ranged from 0.97 to 1.73. The R^2 value was 0.60, and the *p*-value was <0.0001. This indicated that the fractural lesion that showed an initial SUV of 40

displayed a decrease in SUV of 4.6 per 30 days, SUV=30 decreased by 3.1 per month, and SUV=20 decreased by 1.6 per month.

For degenerative lesions, the formula was as follows :

 $\Delta SUVmax30d = -0.04 \times preSUVmax + 0.62.$

With this formula, the 95%CI of the slope was -0.06 to -0.03, and the intercept ranged from 0.33 to 0.92. The R^2 value was 0.09, and the *p*-value was <0.0001.



Figure 2. Scatterplot of lesion SUV_{max} on the first scan (preSUV_{max}) and the rate of change in SUV_{max} standardized to 30 days ($\Delta SUV_{max}30d$). Fractural lesions (**F**) are shown as red circles, and degenerative lesions (**D**) are shown as blue triangles. Red (**F**) and blue (**D**) lines illustrate linear regression. Horizontal dot line indicates $\Delta SUV_{max}30d$ =0. Note that the horizontal axis of preSUV_{max} uses a logarithmic scale

Differentiation between fracture and degeneration

Figure 3 illustrates the ROC curves to differentiate fractural lesions from degeneration. Table 3 summarizes the AUC of

the ROC and other statistical data for differentiating fractures from degeneration in all cases and in the five groups divided according to $preSUV_{max}$.



Figure 3. Receiver operating characteristic analyses to discriminate fracture from degeneration by Δ SUV_{max}30d. Diagonal red dotted lines represent non-discriminatory tests

Table 3. Summary of statistica	l data on differentia	l ability by preSUV _{max}
--------------------------------	-----------------------	------------------------------------

	All cases	30≤ PreSUV _{max}	20≤ PreSUV _{max} <30	15≤ PreSUV _{max} <20	10≤ PreSUV _{max} <15	PreSUV _{max} <10
Area under the curve (95%CI)	0.73 (0.67–0.78)	0.89 (0.77–1.00)	0.86 (0.78–0.95)	0.80 (0.67–0.94)	0.91 (0.86–0.98)	0.59 (0.47–0.71)
Median $\Delta SUV_{max}30d$ on fracture	-0.62	-4.10	-2.24	-1.16	-0.60	-0.04
Median $\Delta SUV_{max}30d$ on degeneration	-0.04	-1.50	-0.33	-0.14	-0.03	0.10
P values	<0.0001	<0.001	<0.0001	<0.0001	<0.0001	0.14
Number of fractures	157	16	23	20	46	52
Number of degenerations	266	13	50	54	105	44

Discussion

Utilizing quantitative SPECT/CT, we evaluated the natural course of bone metabolic activity in fractural and degenerative lesions using SUV_{max}. We found that the SUV_{max} of fracture decreased significantly earlier than that of degeneration, which may offer a key characteristic for discriminating between these pathologies. The significance of the present study is that we

quantitatively demonstrated the possibility of determining whether a lesion showing increased uptake represents fracture after a certain period when encountering such cases.

The uptake on fractural lesions gradually decreased at a constant rate, whereas degenerative lesions appeared to show relatively little change. Although not included in this study, malignant bone tumors, including metastases, without any treatment are expected to increase the uptake in a short period, further facilitating discrimination between them.

We evaluated the rate in SUV_{max} over time and standardized the changes to 30 days as Δ SUV_{max}30d. The Δ SUV_{max}30d was significantly higher for fractural lesions than for degeneration, and these findings were consistently observed in groups with 10≤ SUV_{max}. While no significant difference between values was identified for the group with SUV_{max} <10, such SUVs can be considered to reflect physiological or near-physiological uptake.

Inverting the approximate equation in fractural lesions, the $\Delta SUV_{max}30d$ was estimated as around zero when preSUV_{max} was 9. A previous paper reported that the SUV_{max} of normal bone is approximately 5–10 (12-14), generally consistent with our findings.

We can find a lot of positive numbers of Δ SUV_{max}30d in Figure 2, which indicates uptake increase after follow-up, in fractures and degeneration in which SUV_{max} was around 10 or less. Such results may indicate that Δ SUV_{max}30d is converging to zero. On the other hand, some combinations take an extremely high positive Δ SUV_{max}30d among them. Such values may suggest that a fractural site has re-fractured and is showing even more increased accumulation. Once fractured, these fragile areas could be re-fractured by minor stressors such as coughing or trauma (15).

Detailed interviews with the patients are indispensable to understand the pathological condition. There seem to be more certain technical errors in the quantification of SPECT/CT than in PET, but these errors are generally considered within the permissible range (16). Moreover, Arvola et al. reported that SUVs of SPECT/CT and PET/CT with ¹⁸F-NaF are quite similar (12).

We used 30 days for standardization because this is easy to understand as a quantitative value, but we should note that this study did not evaluate actual data from a 30-day period for reference. A more extended period may be required to assess changes, or determination over a shorter period may be feasible. Additional prospective studies are necessary to clarify the optimal timings in the future.

We consider the present study had some limitations. First, final diagnoses were not based on pathological results, but rather on visual diagnoses by expert nuclear medicine physicians. Decisions in the present study could thus have included some misdiagnosed pathologies. Second, this study did not include any malignant bone lesions. Differentiating bone metastasis from benign fracture is clinically essential, but adding metastatic lesions into this kind of analysis would not be easy, because such metastatic lesions should be treated immediately. Modification of the uptake by treatment cannot be excluded in this analysis. Third, some of the combinations included relatively long periods between scans.

After a certain point, uptake stops changing, which would introduce errors into the calculation. In this study, the maximum interval between scans was 886 days, and we cannot exclude the possibility of underestimating the change in such cases. And finally, we evaluated several types of fractures together. The healing process of a fracture includes an inflammatory phase, a reparative phase, and a remodeling phase (17), and the tracer accumulation of bone scintigraphy varies according to these phases.

Therefore, it is important to evaluate separately by the exact injury time and the type of fracture or location.

Conclusion

Quantitative SPECT/CT depicted the natural time course of bone metabolic activity on fracture and degeneration by SUV_{max}.

 SUV_{max} decreased significantly earlier for fracture than for degeneration.

Acknowledgments

The authors would like to thank Forte, Inc. (www.fortescience.com) for English language editing. No potential conflicts of interest were disclosed.

References

- 1. Corcoran RJ, Thrall JH, Kyle RW, Kaminski RJ, Johnson MC. Solitary abnormalities in bone scans of patients with extraosseous malignancies. Radiology. 1976; 121(3Pt 1):663-7.
- 2. Matin P. The appearance of bone scans following fractures, including immediate and long-term studies. J Nucl Med. 1979; 20(12):1227-31.
- 3. Lee WW. Clinical Applications of Technetium-99m Quantitative Single-Photon Emission Computed Tomography/ Computed Tomography. Nucl Med Mol Imaging. 2019; 53(3):172-81.
- Ross JC, Vilić D, Sanderson T, Vöö S, Dickson J. Does quantification have a role to play in the future of bone SPECT? Eur J Hybrid Imaging. 2019; 3(1):8.
- 5. Kangasmaa TS, Constable C, Sohlberg AO. Quantitative bone SPECT/CT reconstruction utilizing anatomical information. EJNMMI Phys. 2021; 8(1):2.

Yamane T et al

- 6. Miyaji N, Miwa K, Tokiwa A, Ichikawa H, Terauchi T, Koizumi M, et al. Phantom and clinical evaluation of bone SPECT/CT image reconstruction with xSPECT algorithm. EJNMMI Res. 2020; 10(1):71.
- 7. Kuji I, Yamane T, Seto A, Yasumizu Y, Shirotake S, Oyama M. Skeletal standardized uptake values obtained by quantitative SPECT/CT as an osteoblastic biomarker for the discrimination of active bone metastasis in prostate cancer. Eur J Hybrid Imaging. 2017; 1(1):2.
- Hata H, Kitao T, Sato J, Asaka T, Ohga N, Imamachi K, et al. Monitoring indices of bone inflammatory activity of the jaw using SPECT bone scintigraphy: a study of ARONJ patients. Sci Rep. 2020; 10(1):11385.
- Kobayashi Y, Okui T, Tsujimoto M, Ikeda H, Satoh K, Kanamori D, et al. Effect of morphological findings in computed tomography on the quantitative values in single-photon emission computed tomography for patients with antiresorptive agent-related osteonecrosis of the jaw: a cross-sectional study. Ann Nucl Med. 2021; 35(7):853-60.
- Yamane T, Kuji I, Seto A, Matsunari I. Quantification of osteoblastic activity in epiphyseal growth plates by quantitative bone SPECT/CT. Skeletal Radiol. 2018; 47(6):805-10.
- 11. Dittmann H, Kaltenbach S, Weissinger M,

Fiz F, Martus P, Pritzkow M, et al. The Prognostic value of quantitative bone SPECT/CT before ²²³Ra treatment in metastatic castration-resistant postate cancer. J Nucl Med. 2021; 62(1):48-54.

- Arvola S, Jambor I, Kuisma A, Kemppainen J, Kajander S, Seppänen M, et al. Comparison of standardized uptake values between ^{99m}Tc-HDP SPECT/CT and ¹⁸F-NaF PET/CT in bone metastases of breast and prostate cancer. EJNMMI Res. 2019; 9(1):6.
- Huang K, Feng Y, Liu D, Liang W, Li L. Quantification evaluation of ^{99m}Tc-MDP concentration in the lumbar spine with SPECT/CT: compare with bone mineral density. Ann Nucl Med. 2020; 34(2):136-43.
- 14. Kaneta T, Ogawa M, Daisaki H, Nawata S, Yoshida K, Inoue T. SUV measurement of normal vertebrae using SPECT/CT with Tc-99m methylene diphosphonate. Am J Nucl Med Mol Imaging. 2016; 6(5):262-8.
- 15. Katrancioglu O, Akkas Y, Arslan S, Sahin E. Spontaneous rib fractures. Asian Cardiovasc Thorac Ann. 2015; 23(6):701-3.
- 16. Yamane T, Fukushima K, Shirotake S, Nishimoto K, Okabe T, Oyama M, et al. Testretest repeatability of quantitative bone SPECT/CT. Ann Nucl Med. 2021;35(3):338-46.
- 17. Cottrell JA, Turner JC, Arinzeh TL, O'Connor JP. The Biology of Bone and Ligament Healing. Foot Ankle Clin. 2016; 21(4):739-61.